**NANOSPONGES: A DRIVEN APPROACH FOR NOVEL DRUG DELIVERY**

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**ABSTRACT**

A dynamic and multidisciplinary discipline, nanotechnology encompasses a wide range of generically diverse fields, including nano-electronics, information technology, biotechnology, and cellular and molecular biology. Additionally, it has had a significant impact on the development of biomaterials as well as drug delivery, diagnostics, nutraceuticals, and other aspects of the life sciences. Items that are nanosized and can be modified into many approaches to enhance their qualities to make up pharmaceutical nanotechnology. Targeted drug distribution can be accomplished with the help of nanosponges. Numerous medicines, both hydrophilic and lipophilic, can be employed into nanosponges to deliver drugs to specific areas., improving the drug's solubility and bioavailability in the process. As soon as they come into contact with the particular target site, interact, adhere to the surface, and start to release the medicine in a controlled manner, nanosponge can circulate throughout the entire body. Application of nanosponges, types, preparation techniques, polymers employed, and characterization have all been covered in this review paper.

**Keywords: Nanotechnology, Nanosponges, Cyclodextrin**

1. **INTRODUCTION**

The "Pharmaceutical Nanotechnology" a subfield of medicinal research, provides novel tools, opportunities, as well as research directions that are anticipated to have important consequences for the diagnosis and treatment of disease. Nanotechnology is broadly described as "the manipulation of matter on an atomic, molecular, and supramolecular scale including the design, manufacture, specification, and utilization in a several fields offering advanced technical improvements, primarily in the medical field. Nanotechnology has the potential to have an impact in many areas of medicine, such as immunology, cardiology, endocrinology, ophthalmology, cancer, and pulmonology, among others. Additionally, it is widely used in specialized fields like gene delivery, tumor targeting, and brain targeting.[1]. Nanotechnology had dominated technology since the 1950s. In 1959, Richard P. Feynman, a researcher at Cal Tech, predicted something about nanomaterials. He remarked, "There is plenty of room at the bottom," and offered the idea that scaling down to the nanoscale and beginning at the very bottom became the key to future advancements in nanotechnology. Nanomaterials are defined as substances having minimum one dimension between 1 and 100 nm. Nanoscale materials have been developed and used by the pharmaceutical and healthcare sectors to address a variety of physical, chemical, and biological issues related to the treatment of disease. Nanoparticles have a wide range of uses, including the creation of biocompatible materials, the UV protection of textiles, coatings to prevent microbial growth, the delivery of drugs and DNA, the immobilization of enzymes, etc. Several nanosystems have been developed till date, including micellar systems, dendrimers, solid-lipid nanoparticles, carbon nanotubes, polymeric nanoparticles, nanoemulsions, and nanosponges.[2].

The types of nanoparticles can be categorized based on their interaction with medications.

1. Encapsulating Nanoparticles: Particulate systems such as Nanosponges and nanocapsules are examples of this class. Alginate nanosponges, sponge-like nanoparticles having many holes for distributing drug components, are examples of nanosponges. Nanoparticles are also enclosed in nanocapsules made of poly (isobutyl cyanoacrylate, or IBCA). They have an aqueous core where drug molecules can be trapped.
2. Complexing Nanoparticles: These particles attract molecules by electrostatic charges and fall under the category of complexing nanoparticles.
3. Conjugating Nanoparticles: Covalent linkages connect these conjugating nanoparticles to pharmaceuticals.[3].

Recently, nanosponges have been created and are being considered for drug delivery. Nanosponges have the ability to delay the enhance the bioavailability of medications that aren't easily dissolved in water. Because of their inner hydrophobic chambers and external hydrophilic branches, nanosponges have unrivaled flexibility and is capable of transporting both hydrophilic as well as hydrophobic medicinal molecules. Nanosponges resemble a three-dimensional scaffold or network more so. Figure 1 illustrates a nanosponge, which is a small mesh-like structure that may be utilized to incorporate a variety of ideas of different compounds.[4,5]. Their spherical colloidal nature has been established, and their inclusion as well as non-inclusion behavior indicate that they have an extremely high rate of solubilization for insoluble medicines.[6]. The polymer's lengthy polyester backbone is combined in solution with smaller molecules which are referred as cross-linkers to serve as a tiny grappling hook for joining the various components of the polymer.[7].

1. **ADVANTAGES** [4,8]
2. These compositions maintain their stability between pH 1 and 11.
3. These compounds maintain the stability at elevated temperatures.
4. These compositions work well with the majority of substances and vehicles.
5. Due to their usual 0.25 m pore size, they are self-sterilizing and prevent germs from growing.
6. These formulations may be inexpensive and flexible.
7. This approach gives greater formulation flexibility, increased elegance, higher stability, less negative consequences, and component trapping.
8. Nanosponges are neither mutagenic, poisonous, or allergic.
9. Activities with extended release that last up to 12 hours are feasible.
10. Allows the addition of immiscible liquid; improves material processing by turning liquid into powder.
11. Commercial production scaling up is easy.
12. The cross-linker to polymer ratio can be varied to alter the size of the nanosponges.
13. Depending on the required dose, the medication's release characteristics may be quick, medium, or slow.
14. An anticipated release.
15. Nanosponges can be renewed by adjusting the pH or ionic strength, light heating, washing with eco-friendly solvents, or stripping with comparatively inert hot gases.
16. Less harmful side effects as a result of less frequent drug contact with healthy tissue.
17. **DISADVANTAGES** [9]
18. Nanosponges can only incorporate extremely small molecules.
19. Crystalline or paracrystalline nanosponges are also possible.
20. The loading ability of nanosponges is mostly determined by the degree of crystallization.
21. Paracrystalline nanosponges have various loading capabilities.
22. **CHARACTERISTIC OF NANOSPONGES** [11]
23. Nanosponges offer a variety of diameters (1 m or less) with adjustable cavity polarity.
24. By altering the cross-linker to polymer ratio, nanosponges of a particular size can be created.
25. They can appear crystalline or paracrystalline, depending on the conditions of the operation. The crystal structure of nanosponges is crucial in ensuring the complexation of medications with them.
26. The drug loading capacity is determined by the degree of crystallization.
27. Paracrystalline nanosponges have a variety of drug loading capacities.
28. They have porous components that are nontoxic, largely insoluble in organic solvents, as well as stable up to 300 °C.
29. They can withstand pH levels between 1 and 11.
30. In water, they create a clear, opalescent suspension.
31. They can be duplicated utilizing straightforward thermal desorption, solvent extraction, microwaves, and ultrasounds.
32. Several compounds can be captured, transported, and released under regulated conditions due to their 3D designs.
33. Because of their ability to connect with several functional groups, they can be placed at various target places.
34. Nanosponges can connect more effectively to the target region thanks to chemical linkers.
35. Nanosponges are capable of forming inclusion- as well as non-inclusion-based complexes when they interact with certain medicines.
36. Magnetic qualities can also be given to nanosponges by including magnetic particles in the reaction mixture.
37. Nanosponges are porous, highly soluble in water particles that are primarily employed to encapsulate poorly soluble medicines.
38. These Nanosponges may transport both hydrophilic and lipophilic medications.
39. They are able to filter out organic contaminants from water and guard against physicochemical deterioration, which would otherwise destroy the medicine.
40. **TYPES OF NANOSPONGES**

**Figure 2:** Types of Nanosponges

**Cyclodextrin Nanosponges:**

The term "cyclodextrin nanosponges" (CDNS) was initially introduced by DeQuan Li and Min Ma in 1998 to describe a cross-linked -cyclodextrin with organic di-isocyanates that results in the creation of a network that is not soluble and indicates a higher inclusion constant with diverse organic contaminants. A new drug delivery system for nanoscales called CDNS is proposed. It consists of a three-dimensional network of cross-linked polymers of cyclodextrin nanostructure. By altering the cross-linker and degree of cross-linking, CD polymer are able to produce spherical, crystalline, or amorphous, porous, insoluble nanoparticles with tunable polarity and size. There are three distinct CD types: Three different kinds of cyclodextrin exist: Alpha-cyclodextrin (α) Beta-cyclodextrin (β) Gamma-cyclodextrin(γ) Delta-cyclodextrin(δ), the 3 natural CDs, α-, β- and γ- CDs, having different ring size and solubility.[12,13].

A unique nanostructured material made of hyper-cross-linked cyclodextrins has been described which is produced by reaction of cyclodextrins (cyclic oligosaccharides) along with suitable cross-linking reagents. This material is known as nanosponges.[14]. Depending on the agent utilized as a cross-linker, nanosponges can be created as neutral or acidic materials and can swell. The end result leads to the development of spherically shaped particles which has cavities that can hold medicinal molecules.[15].



**Figure 1.** Cyclodextrin carbonates nanosponges' molecular structure.

During preparation, the cross-linking-to-cyclodextrin ratio can be changed to enhance drug loading and create a customized release profile.[15,16]. Compared to the parent cyclodextrin molecules, the extremely porous of nanosponges and the nanomeric nature allows drug molecules to orient themselves in the inclusion of the nanosponge as well as interact in a non-inclusion form.[16]. Comparing nanosponges to ordinary nanoparticles reveals a striking benefit. They are in fact easily regenerable using a variety of processes, including washing with environmentally friendly solvents, stripping with relatively inert hot gases, gentle heating, or altering pH or ionic strength. Nanosponges have previously been used in a variety of applicable domains, including the cosmetic and pharmaceutical industries, due to all these qualities.[7].

The nanosponges are physically solid in nature.[17]. They are safe for both oral and invasive routes, making them a viable medication delivery vehicle.[18]. Owing to their small size, nanosponges can be delivered through the lungs and veins. The complexes can be dissolved in a mixture of excipients, diluents, lubricants, as well as anti-caking agents that are suitable for making tablets or capsules for oral administration. Saline, sterile water, and other aqueous solutions can all be used to carry the substance and deliver it by parenteral injection. In order to distribute drugs topically, they can be effectively incorporated into topical hydrogel. The medication molecules are contained within the center of encapsulating nanoparticles called nanosponges.[19].

 Cyclodextrins have been primarily used in the pharmaceutical industry because,

1. They are semi-natural goods made by relatively simple enzymatic conversion from renewable natural starch.
2. They are created using environmentally friendly methods at a rate of thousands of tons annually.
3. Any hazardous effects they may have are of a minor kind and can be completely avoided by using the proper cyclodextrin type, derivatives, or application method.

**Additional classifications of CD-based Nanosponges include:**

1. CD-based carbamate nanosponges:

In the presence of a DMF solution, CDs reacts with appropriate di-isocyanates, like hexamethylene di-isocyanate and toluene-2, 4-diisocyanate, for 16 to 24 hours at 70 °C under a nitrogen environment. By thoroughly washing with acetone, residual DMF is eliminated, and cross-linked polymer powder is produced. These nanosponges are used to purify water because of their capacity for binding to organic compounds. For organic compounds, the loading capacity varies between 20 to 40 mg per cm3.[20,21].

1. CD-based carbonate nanosponges:

Active carbonyl compounds like CDI, DPC, and tri-fosgene are the primary cross-linkers used to manufacture this sort of nanosponges. Two CD monomers form carbonate bonds in the resultant CD nanosponges. If a solvent is present or absent, the reaction can be conducted at ambient temperature or between 80 and 100°C using either the melt technique or the solvent approach. The polarity and cavity diameters of carbonate-CD based nanosponges can be changed, which is one of their key properties. They can be produced under various conditions to yield various shapes, such as amorphous or semi-crystalline. Numerous medications, including paclitaxel, camptothecin, dexamethasone, flurbiprofen, 5-fluorouracil, cilostazol, progesterone, oxcarbamazepine, nelfinavir mesylate, resveratrol, and tamoxifen, have been encapsulated using carbonate-CD-based nanosponges. Water's surface tension is not considerably impacted by carbonate nanosponges. Due to their non-hygroscopic nature, they preserve their crystal structure both during the process of absorption of moisture and desorption. The ability of CD-based carbonate nanosponges to increase the level of solubility depends heavily on their level of crystallinity, which is a distinctive characteristic.[7, 21].

1. CD-based ester nanosponges:

The crosslinking agent employed to create these nanosponges is a suitable dianhydride, such as pyromellitic anhydride. The CD and dianhydride are dissolved in DMSO in the presence of an organic base, such as pyridine or triethylamine (to speed the reaction in a forward direction), to perform the exothermic crosslinking process, which is carried out at room temperature and is very quick (finished in a few minutes). A polar free carboxylic acid group found in these nanosponges allows them to accommodate cations as well as apolar organic molecules concurrently.[22].

1. Polyamidoamine Nanosponges:

Polyamidoamine nanosponges are made by performing the reactions in the water. After 94 hours at room temperature of prolonged standing, CD polymerizes with acetic acid 2, 20-bis (acrylamide). They have acidic and basic residues, which causes them to swell in water (pH dependant behaviour). When the polymer comes into contact with water, a translucent gel forms immediately. The stability of the gel for up to 72 hours was validated by time-dependent swelling experiments in biorelevant medium. Albumin was used in the studies as a model protein because of its extremely high encapsulation efficiency—roughly 90%. Studies on in vitro drug release demonstrated that the protein release may be controlled for up to 24 hours. The stability of the product was examined using the sodium dodecyl sulfate (SDS) PAGE method. SDS PAGE analysis of the protein's conformational stability revealed that the formulation was stable for up to many months.[23].

1. Modified Nanosponges:

Traditional carbonate-based nanosponges have been modified to better suit the application by changing the reaction conditions. Fluorescein isothiocyanate was combined with carbonate nanosponges in DMSO and heated to 90 °C for a few hours to produce the fluorescent derivative. Fluorescent nanosponges have been employed in biological research, including the treatment of cancer. A cyclic organic anhydride like succinic anhydride or maleic anhydride can be used in a similar way to produce carboxylated nanosponges. Such nanosponges react with proteins, chitosan, or other biologically significant carriers, perhaps resulting in a promising medication targeting action for a particular receptor. These nanosponges are amorphous by nature, according to powder XRD measurements. They are not cytotoxic or hemolytic either. Carboxylated nanosponges seem to offer a viable safe drug delivery system for anti-cancer medications like camptothecin.

1. **DRUG RELEASE MECHANISM FROM NANOSPONGES**

Up until equilibrium is attained, the sponge atoms are in an open state, permitting the molecules that are active to freely enter and leave the particles as well as the vehicle. In the case of topical distribution, the chemical component that is already present in the vehicle will eventually be absorbed into the target tissue after being administered to it. When a vehicle is depleted, the equilibrium is thrown off because the vehicle will become unsaturated. As a result, an active flow will start from the sponge particle in the vehicle and continue until the vehicle is either dried out or absorbed before moving from the vehicle to the target tissue. The sponge fragments that remained on the tissue's surface would then continue to slowly release the active substance to it, giving the tissue a sustained release over time.[4].

1. **METHODS OF PREPARATION OF NANOSPONGES**
2. **Solvent method**

The polymer was combined using an appropriate solvent in this approach, specifically a polar aprotic solvent like di-methylformamide or di-methylsulfoxide. This combination was added to extra cross-linker, particularly in a 4 to 16 molar ratio between the cross-linker and the polymer. The reaction was run for 1 to 48 hours at temperatures varying from 10 °C upto the solvent's reflux temperature. Dimethyl carbonate as well as carbonyl di-imidazole are preferred cross linkers among carbonyl compounds. After the reaction was finished, the solution was allowed to cool at ambient temperature. Then, the product was added to a significant amount of bidistilled water, which was then filtered under vacuum to recover the product, which was then further purified by prolonged Soxhlet extraction with ethanol. The product was vacuum-dried before being mechanically milled to create a uniform powder.[7].

1. **Ultrasound-assisted synthesis**

Using this technique, nanosponges were developed by combining cross-linkers and polymers without the need of a solvent which was being sonicated. Spherical, uniform-sized nanosponges will be created using this method. The cross-linker along with polymer were mixed in a flask at a specific molar ratio. The flask was placed in an ultrasonic bath with water and heated to 90 °C. 5 hours were spent sonicating the mixture. After allowing the mixture to cool, the final product was roughly broken. After being thoroughly cleaned with water to get rid of the non-reacted polymer, the product underwent a lengthy Soxhlet extraction in ethanol. The finished product was vacuum-dried and kept in storage at 25 °C until needed.[6].

1. **Emulsion solvent diffusion method**

Ethyl cellulose and polyvinyl alcohol are used in various concentrations to make nanosponges. To enhance drug loading and to achieve a customized release, different ratios of medication to polymer are utilized. A specific amount of polyvinyl alcohol in 100 ml of an aqueous external phase was added slowly over the course of three to five hours using a magnetic or mechanical stirrer with the speed of 1000 to 1500 rpm while the dispersion phase, which contained the drug and polymer, was dissolved in 20 ml of dichloromethane. The created nanosponges were filtered out, dried in an oven at 40°C for 24 hours, and then packaged.[6].

1. **From hyper cross- linked β-cyclodextrin**

In this case, cyclodextrin can serve as a medication delivery vehicle. Cyclodextrin and a cross linker can be used to create nanosponges. As a result, 3D networks are created, which might be a somewhat spherical structure with pores and channels inside that is the size of a protein. Sponge size is regulated by porosity and surface charge density for its attachment to various molecules when cyclodextrin reacts with a cross linker such di-isocyanates, diary carbonates, etc. In neutral or acid forms, nanosponges can be created. The typical diameter of a nanosponge is less than 1 m, however fractions as small as 500 nm can be chosen. They are used to improve the solubility of weakly water-soluble medicines in aqueous solutions. They are composed of solid components that have been crystallized.[14].

1. **Polymerization**

Aqueous phase, typically comprising surfactant and dispersant to enhance suspension, is added to a non-polar drug solution created in the monomer. Once the suspension with the distinct droplets of the correct size is developed, by catalyzing or increasing temperatures in order to activate the monomers, polymerization is done. The polymerization process results in a reservoir-like system which opens via holes at the surface.

1. **LOADING OF DRUG INTO NANOSPONGES**

The goal of pre-treating nanosponges for drug delivery is to achieve a mean particle size of less than 500 nm. The nanosponges were subjected to ultrasound while remaining suspended in water to prevent the formation of aggregates. The colloidal fraction was then obtained by centrifuging the solution. After the supernatant was separated, the product was dried using a freeze-drying process. The extra medication was diluted into the nanosponges' aqueous suspension, and the mixture was constantly stirred for the specified amount of time to allow for complexation. Centrifugation has been used to separate the complexed medicine from the uncomplexed (undissolved) drug after complexation. The solid nanosponges crystals were then made by freeze drying or solvent evaporation. The crystal structure of the nanosponge is essential for the complexation of medicines. Paracrystalline and crystalline nanosponges possess distinct loading capacities, according to a study. Drug loading is higher in crystalline nanosponges than paracrystalline ones. In weakly crystalline nanosponges, drug loading occurs as a mechanical interaction instead of an inclusion complex.[7].

1. **CHARACTERIZATION OF NANOSPONGES**
2. **Particle size determination:**

An essential consideration in the nanosponge optimization process is the particle size. Both the drug's solubility and release can be impacted by the drug's particle size. Particle size can be determined using a Zeta sizer or laser light diffractometry.[24]. Plotting the cumulative percentage drug release from nanosponges with different particle sizes against time allows researchers to examine how particle size affects drug release. Particle sizes ranges from 10 and 25 µm may be desirable for topical medication administration, whereas those more than 30 µm may exhibit a gritty sensation.[27].

Babchi oil is encapsulated in herbal formulations using cyclodextrin-based nanosponges. They used five different varieties of babchi oil that were infused with different molar ratios of cyclodextrin nanosponges. The BO nanosponges' particle sizes ranged from 234 to 484 nm (table no 1). The particle sizes of each of the prepared BO nanosponges were in the nano range (1 nm). This shows they are in significant range.[28].

**Table no. 1**

|  |  |  |
| --- | --- | --- |
| **Sr.no** | **Formulation** | **Particle size (nm±SD)** |
| 1 | BONS1:2 | 261.6±14.79 |
| 2 | BONS1:4 | 360.9±11.55 |
| 3 | BONS1:6 | 234.3±15.37 |
| 4 | BONS1:8 | 484.2±19.89 |
| 5 | BONS1:10 | 243.3±12.95 |

In synthetic the characterization of carboxymethyl chiton nanosponges with cyclodexin blends were studied to check drug solubility increases or not. The produced nanosponges' average particle sizes (F-0 to F-9) are displayed (table no 2). The particle sizes of all the manufactured nanosponges were in the nano range (1 nm). This shows they are in significant range.[29].

**Table no 2**

|  |  |  |
| --- | --- | --- |
| **Sr.no** | **Formulation** | **Particle size (nm)** |
| 1 | F0 | 195±3 |
| 2 | F1 | 213±2 |
| 3 | F2 | 238±5 |
| 4 | F3 | 250±4 |
| 5 | F4 | 224±3 |
| 6 | F5 | 209±4 |
| 7 | F6 | 211±4 |
| 8 | F7 | 218±3 |
| 9 | F8 | 205±4 |
| 10 | F9 | 199±5 |

1. **Polydispersibility index (PDI):**

The polydispersibility index (PDI) is a measure of the spread or width of the particle size distribution and it reveals variation within it. To calculate PDI, a dynamic light scattering device is employed.[24]. A higher PDI value implies that the sample has a wider particle size distribution and is polydisperse, whereas a monodisperse sample has a lower PDI. PDI may be computed using the equation below.[27,30].

**PDI = d/d avg ∆**

Where,

**d** is the width of distribution denoted by **SD**, and **d Avg** is the average particle size denoted by MV(nm) in particle size data sheet.

**Table no 3**

|  |  |
| --- | --- |
| **Polydispersibility index** | **Type of dispersibility** |
| 0-0.05 | Monodisperse standard |
| 0.05-0.08 | Nearly monodisperse |
| 0.08-0.7 | Mid-range polydisperse |
| >0.7 | Mid-range polydisperse |

After accurately establishing the initial weight of the raw materials and the final weight of the produced nanosponge, the production yield of the nanosponges may be estimated using the equation below.[30].

**Production yield (PY) = Practical mass of NS ÷ Theoretical mass (polymer + Drug) × 100**

As reported cyclodextrin was encapsuled by babchi oil to study the cytotoxicity study and characterization of herbal formulation. They have taken five types of babchi oil which is loaded by Cyclodextrin Nanosponges in Different molar ratio (table no 3). The stability and homogeneity of the nanocolloidal suspensions were demonstrated by reduced PDI values with a constrained range(table ). All of the nanoformulations were discovered to be fine, free-flowing powders.[29].

**Table no 4**

|  |  |  |
| --- | --- | --- |
| **Sr.no** | **Formulation** | **Polydispersity Index ± SD** |
| 1 | BONS1:2 | 0.312 ± 0.098 |
| 2 | BONS1:4 | 0.311 ± 0.059 |
| 3 | BONS1:6 | 0.188 ± 0.064 |
| 4 | BONS1:8 | 0.509 ± 0.236 |
| 5 | BONS1:10 | 0.361 ± 0.113 |

As reported cyclodextrin was encapsuled by babchi oil to study the cytotoxicity study and characterization of herbal formulation. They have taken five types of babchi oil which is loaded by Cyclodextrin Nanosponges in Different molar ratio (table no 3). The stability and homogeneity of the nanocolloidal suspensions were demonstrated by reduced PDI values with a constrained range (table ). All of the nanoformulations were discovered to be fine, free-flowing powderS.[29].

1. **Zeta potential:**

By measuring the surface charge of Nano sponges using a tool called a zeta sizer, one may determine the zeta potential. For measuring the Zeta potential and the magnitude of the electrical surface charge at the double layer is frequently utilized. Zeta potential values greater than 30 mV signify strong formulation stability.[31].

During encapsulation of babchi oil to study physiochemical and characterization with cyclodextrin based nanosponges. They have taken five types of babchi oil which is loaded by Cyclodextrin Nanosponges in Different molar ratio (table no 4). As a gauge of surface charge, the zeta potential of several BO nanoformulations was also examined. The acquired zeta potential data are reported and are in significant range i.e ±30mV a steady nanosponge is indicated by a high zeta potential because of stronger repulsive forces, which reduces their propensity to assemble.[28].

**Table no 5**

|  |  |  |
| --- | --- | --- |
| **Sr.no** | **Formulation** | **Zeta Potential (mV ± SD)** |
| 1 | BONS1:2 | −17.8 ± 2.52 |
| 2 | BONS1:4 | −16.0 ± 1.15 |
| 3 | BONS1:6 | −15.5 ± 1.17 |
| 4 | BONS1:8 | −15.6 ± 2.39 |
| 5 | BONS1:10 | −22.0 ± 2.47 |

To study synthesis and characterization of nanosponges CDI cross-linked with β-cyclodextrin,

F1 and F2 were discovered to have zeta potentials of -14.2 mV and -8.74 mV, respectively.[23].

1. **Thermodynamical method:**

To determine whether drug molecules or particle modifications occur prior to the heat destruction of Nano sponges, the thermo-chemical technique may be applied. Only a few of the many potential drug particle modifications include melting, evaporation, oxidation, breakdown, and polymeric modifications. Changes in the drug molecules indicate the formation of a potent compound.[31].

In herbal formulation of babchi oil which was encapsuled in cyclodextrin to study characterization, in vitro cytotoxicity and physiochemical. Differential thermal analysis measures the temperature difference between the sample and the reference that led to heat absorption or release.[28]. Carboxymethyl was encapsuled in cyclodextrin blends to improve drug solubility. Overall, the findings of the DSC and TGA investigations demonstrated that bi-polymeric nanosponges were successfully formed, and that thermal stability was improved.[29].

1. **Microscopy studies:**

Examining the microscopic components of a medication or nanosponge formulation can be done using either scanning electron microscopy (SEM) or transmission electron microscopy (TEM). By using SEM to analyze the morphology of nanosponges, it is possible to determine if inclusion complexes have formed between the raw materials utilized to create a nanosponge and the formulation's ultimate crystallization state.[31].

The loading efficiency (%) of Nanosponge can calculate by using following equation:

**LE = Actual drug content in nanosponges ÷ Theoretical drug content x 100**

Loading efficiency may also be assessed using an HPLC method and an empirical evaluation of the medication placed in a nanosponge ultraviolet spectrophotometer. This entails counting the number of drug-loaded nanosponges that have been dispersed in appropriate solvent and broken up any complexes using a sonicator for a certain period of time. Following dilution, the sample is analyzed with an HPLC or UV spectrophotometer.[32].

In formulation for herbal babchi oil was encapsuled in cyclodextrin**.** They have taken five types of babchi oil which is loaded by Cyclodextrin Nanosponges in Different molar ratio.For the babchi oil NS, it was discovered that BONS4 had the maximum encapsulation efficiency up to 93% while BONS10 had the lowest just 61%.A larger amount of oil can be encapsulated in the nanosponge matrix and a cyclodextrin cavity due to optimal crosslinking that involves inclusion and external contacts simultaneously. This may explain why the BO is more fully encapsulated in a 1:4 molar ratio.[28].

Enhancing Drug Solubility using Carboxymethyl Chitosan Nanosponges and Cyclodextrin Blends were being synthesized and characterized. All of the findings, namely those between 85.32 and 87.4% and 89.32 and 91.74%, were deemed to be acceptable. All nanosponges displayed drug loading of at least 70%. The minimal Drug-loaded contents and the effectiveness of drug entrapment were shown by batch no F-8 and F-9, respectively, at 71.40-74.44% and 80.43-83.62%. Due to the product's stickiness, lansoprazole-loaded nanosponges displayed lower DLC% with an increase in polymer concentration. Furthermore, due to the low water solubility of the polymer, the drug entrapment efficiency significantly reduced with increasing polymer concentration.[29].

1. **Solubility studies:**

It was explained how Higuchi and Connors created the phase solubility approach to study inclusion complexation. This method was used to explain how the drug's solubility was modified by Nanosponge, which demonstrates the level of complexity.[33].

During study of Itraconazole-Loaded Nanosponges for Topical Drug Delivery for preparation and In-Vitro evaluation. By using the shake flask technique, the solubility of each nanosponge formulation in distilled water and 0.1 N HCl was measured. Itraconazole's solubility increased by around 21 times.[30].

For improving drug solubility via the synthesis and characterization of carboxymethyl chitosan nanosponges with cyclodextrin blends. The outcomes showed that the primary goal of creating nanosponges improving docetaxel's solubility was achieved. Previous research indicated that nanosponges provide the highest solubility improvement for lipophilic medicines. Furthermore, our study showed a much higher drug solubility at pH 6.8 compared to other standard CD nanoparticles. [29].

1. **FTIR spectroscopy:**

The interaction between drug molecules and drug and nanosponge in the solid state is estimated using IR spectroscopy. When a complex between a drug and a nanosponge forms and a little portion of the drug molecule is allocated to include a portion of other molecule that is designated by bands on the spectra of nanosponges, the IR changes. The use of IR for several medications that include carbonyl or sulfonyl groups is restricted. Information on functional groups including drugs is provided via IR studies.[27].

While studying physiochemical characterization, photodegradation, and in vitro cytotoxicity studies of babchi oil encapsulated in cyclodextrin-based nanosponges. The distinctive peaks of the BO were widened or shifted in nanoformulations, which implies interactions between oil and nanosponges, according to a comparison of the FTIR spectra of BO, blank NS, and BONS4.[28].

The spectra of loaded formulations showed a decrease in peak height and intensity as well as a complex formation between the drug and the monomer (AMPS) and polymers (CMC and -CD). These changes also showed slight peak shifting, modification, disappearance, and emergence was reported during study of improving drug solubility of carboxymethyl chitosan nanosponges with cyclodextrin blends.[29].

1. **X-ray diffractometry:**

Using powder X-ray diffractometry, inclusion complexation in the solid state may be identified. The complex manufacturing of the medication using nanosponges changes its diffraction patterns and crystal structure.[27]. A newly created material obviously varies from an uncomplicated nanosponge with regard to of its diffraction pattern, nanosponge. The complex creation is shown by this discrepancy in the diffraction pattern. When a complex forms, the peaks get sharper and a few more peaks develop.[32].

For herbal forumation of babchi oil Significant differences between their diffract grams occur, as evidenced by the observed drop in peak intensity. As a result, according to the XRPD experiments, freeze drying (BONS4) produced a fluffy powder with a highly porous structure that had lost its crystallinity. The indicated temperatures correspond to the typical peaks of the blank nanosponges: 10.53°, 12.37°, 15.14°, 16.99°, 18.60°, 19.29°, 20.92°, 22.52°, 24.15°, 25.30°, 26.90°, 28.52°, 31.05°, 34.75°, 36.60°, and 39.83° (2Ɵ).[28].

During synthetic capsulation the existence of distinctive peaks at 2Ɵ= 11.52º, 13.10º, 15.80º, 20.31º, 22.11º, 23.10º, 26.55º, and 27.71º demonstrated the crystallinity of AMPS. A PXRD diffractogram of a physical combination of medicine and polymer showed fewer but sharper peaks at 2Ɵ = 19.21º, 28.11º, and 36.91º, suggesting that the crystalline character largely diminished. The amorphous system of nanosponges, which is more soluble than the crystalline form of DTX, notably covered the strong distinctive peaks in pure drug DTX in an XRD diffractogram of DTX-loaded CD-co-poly (AMPS) and DTX-loaded CD-CMC-co-poly (AMPS) nanosponges. [29].

1. **In Vitro release studies:**

It is feasible to analyze the drug release from the enhanced nanosponge formulation using a multi-compartment rotation cell with a membrane for dialysis (cut-off 12,000 Da). The donor phase is composed of the drug-loaded nanosponge complex in distilled water. The receptor phase also contains the same media. The receptor phase is completely withdrawn at specified intervals, diluted adequately with distilled water, and then analyzed using a UV spectrophotometer.[27].

The research of itraconazole-loaded nanosponges for topical drug administration uses information from an in-vitro release trial of a chosen batch and a pure medicine. After 120 minutes, it was found that 70.62% of the drug had been released from F4 nanosponges.[30].

During synthetic nanosponges study the drug was within five minutes, drug-loaded nanosponges showed initial abrupt drug release characteristics. After reaching equilibrium in twenty minutes, approximately 99% of the medication was released within one hour. As a result, the study's main goal was accomplished, making it a viable drug delivery method to increase DTX's water solubility, which stood out from other nanotechnologies. The overall findings of our dissolving investigations demonstrate that the quantity and type of the basic reactants utilized have a significant impact on altering the release profile of a medication with poor solubility (docetaxel). When compared to pH 1.2 and 4.5, the drug release of synthesized nanosponges was substantially greater at pH 6.8.[29].

1. **Porosity study:**

A porosity analysis is done to figure ++out how many nanochannels and nanocavities were created. Since helium gas may move via various inter- and intra-specific channels in materials, a helium pycnometer is used to gauge the porosity of nanosponges. The true volume of the substance is determined using the helium displacement method. Nanosponges have higher porosity than the parent polymer used to form the system because they are porous.[34].

**Percent Porosity equation:** **% Porosity (E)= Bulk volume – True volume ÷ Bulk volume × 100**

1. **NANOSPONGE APPLICATIONS**
2. **Solubility enhancement**: Nanosponges can help molecules with very limited water solubility become more soluble and moist. If the drugs are molecularly distributed within the nanosponge structure and then released as molecules, the dissolving process can be avoided. The drug's apparent solubility can be enhanced as a result. Numerous formulation and bioavailability concerns can be overcome by improving a substance's solubility as well as rate of dissolution, and nanosponges can dramatically improve a drug's solubility.
3. **Nanosponges for drug delivery**: One can create dose forms for oral, parenteral, topical, or inhalation use using the nanosponges. They are by definition solid. The complexes can be incorporated into a mixture of excipients, diluents, lubricants, and anti-caking agents that are suitable for making capsules or tablets for oral administration. For parenteral administration, the substance is easily carried in water that is sterile, saline, or other solutions that are aqueous. For topical distribution, they can be effectively incorporated into topical hydrogel.[5].
4. **Topical agents**: A novel method for the controlled release of topical medications of prolong drug release and retention of drug forms on skin is the nanosponge delivery system. Drugs that are easily manufactured as topical nanosponges include local anesthetics, antifungals, and antibiotics. When active substances enter the skin, rashes or more severe adverse effects may develop. In contrast, this technique enables a steady and prolonged rate of release, minimizing discomfort while preserving effectiveness. A designed product includes a wide range of ingredients, including liquid, gel, cream, lotion, ointment, and powder.[16].
5. **Using nanosponges to carry and release enzymes, proteins, vaccines, and antibodies**: Many systems, including nano and microparticles, liposomes, and hydrogels, have been designed to transport proteins and enzymes. Proteins can be stabilized in vivo, have their pharmacokinetics changed by carriage in a specific system, and be protected from deterioration. The ability to adsorb proteins, enzymes, antibodies, and macromolecules is now known to be particularly well suited for cyclodextrin-based nanosponges. When enzymes are utilized, in particular, it is possible to preserve their activity, efficiency, prolong their operation, and expand the pH and temperature range of their activity, which enables the conduct of continuous flow operations. Furthermore, by adsorbing or encasing them in cyclodextrin nanosponges, proteins and other macromolecules can be transported.[36].
6. **Nanosponges as a carrier for delivery of gases:** For both medicinal and diagnostic purposes, gases are utilized in medicine. Numerous disorders, including cancer and inflammatory conditions, are associated with hypoxia, or an inadequate oxygen supply. It might be difficult to give oxygen in the proper form and dosage in clinical settings..[35].
7. **Nanosponges as a barrier against light or deterioration**: Gamma-oryzanol, an ester combination of ferulic acid, has recently attracted a lot of interest because of its potential to serve as a natural antioxidant. In the cosmetics industry, it is frequently used as sunscreen and for preserving food as well as pharmaceutical raw materials. Its application is constrained due to a high degree of instability and photodegradation. Gamma-oryzanol was enclosed in nanosponges, which showed good photodegradation. A gel and an O/W emulsion were produced using the gamma-oryzanol-loaded nanosponges..[36].

**Table 6: A list of drugs complexed by using nanosponge**

|  |  |  |  |  |  |
| --- | --- | --- | --- | --- | --- |
| **Sr. No.** | **Drug** | **Therapeutic Activity** | **Vehicles used in Nanosponges** | **Route of Administration** | **References** |
|  | Curcumin | Anti-neoplastic | β-CD, di-methylcarbonate | Parenteral | [35] |
|  | Acetylsalicylic acid | Anti-inflammatory | β-CD, pyromellitic dianhydride | Oral | [6] |
|  | Resveratrol | Anti-oxidant | β-CD, carbonyldiimidazole | Oral, Topical |  [6] |
|  | Tamoxifen | Anti-estrogen | β-CD, carbonyldiimidazole | Oral | [10] |
|  | 5-Fluorouracile | Antineoplastic | β-CD | Parenteral, Topical | [32] |
|  | Gamma-oryizanol | Antioxidant | β-CD, diphenylcarbonate | Topical | [32] |
|  | Nelfinavir mesylate | Antiviral | β-CD, dimethylcarbonate | Oral | [6] |
|  | Doxorubicin | Antineoplastic | β-CD, diphenylcarbonate | Parenteral | [12] |
|  | Dexamethasone | Anti-inflammatory | β-CD, diphenylcarbonate | Oral, Parenteral | [12] |
|  | Itraconazole | Antifungal | β-CD, copolyvidonum | Oral, Topical | [10] |

1. **PATENTED NANOSPONGES**

**Table 7: List of patented nanosponges**

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
| **Sr. No** | **Title of patent** | **Inventors** | **Year** | **Patent No.** |
| **1.** | Nanosponges as vehicle for antimurol medications | Francesco Trotta, Vander Tumiatti, Roberta Cavalli, Carlo Maria Roggero, Barbaramognetti, Giovanni Nicolao Berta | 2008 | CA2692493A1Canada |
| **2.** | Nanopongess of silicon.. | Declan Farrell, Santosh Limaye Shanthi Subramanian | 2009 | WO2006121870A3WIPO (PCT) |
| **3.** | Nanosponges are used in the transport and release of enzymes, proteins, vaccines, and antibodies, as well as as a biocatalyst carrier. | Gianfranco Gilardi Francesco Trotta,Roberta Cavalli, Paolo Ferruti, Elisabetta Ranucci, Giovanna Di Nardo, Carlo Maria Roggero, Vander Tumiatti | 2009 | WO2009149883A1WIPO (PCT) |
| **4.** | Metal, nanosponge, and a method involving them that are template- and polymer-free | Eswaramoorthymuthusamy, Sai Krishna Katla | 2009 | US8404280B2United States |
| **5.** | Making dextrin nanosponges: the method.. | Francesco Trotta, Pravin Shende, Miriam Biasizzo | 2012 | WO2012147069A1WIPO (PCT) |
| **6.** | An example of a composite sound-absorbing board made with nanosponges. | Li Ligen, Wang Xiaocun | 2017 | CN107498936AChina |
| **7.** | Application of the nanosponge in the field of air purification as well as a technique and tool for processing finely ground particles with negative ion air. | Wang Xiaocun, Wang Zilong | 2017 | CN105180312BChina |
| **8.** | Nanoparticles, nanosponges, synthesis processes, and application techniques. | [Kun Lian](https://patents.google.com/?inventor=Kun+Lian) | 2017 | US20170152439A1United States |
| **9.** | Licoflavone nanosponges and its preparation process | Li Xiaofang, Sun Qiang | 2018 | CN108703944AChina |
| **10.** | Method and preparation of composite of Cu2o And Cu nanosponges. | Liao Jiaxuan, Wu Mengqiang, Xu Ziqiang, Gong Feng,Song Yaochen, Ma Yunfei, Li Shi | 2018 | CN109712817AChina |
| **11.** | A kind of bianry alloy PtCu nanosponges | Yuan Qiang, Hu Yanna,Liu Sun | 2018 | CN108372315AChina |
| **12.** | Materials Based on Cross-Linked Nanoporous Saccharides and Their Fabrication | Wing Nien Wylie O, Tin Lok Li, Zhijian Lin, Dan Cheng, Jifan Li | 2019 | US20210122875A1United States |
| **13.** | Method of making cross linked nanoporous carbohydrate  | Ke Yingnian, Li Tianle, Lin Zhijian, Cheng Dan, Li Jifan | 2019 | CN112469775AChina |
| **14.** | A method for making a nanosponge. | Francesco Trotta, Alberto Rubin Pedrazzo | 2020 | WO2021053039A1WIPO (PCT) |
| **15.** | An etoricoxib loaded nanosponge hydrogel for arthritis & process to prepare thereof | Dr.Ashishyashwantrao Pawar, Dr. Deepak Devidas Sonawane, Dr. Rajendra, Sudhakar Bhambar, Dr. Khanderao Rajaram Jadhav, Kisan Tukaram Pawara, Sejal Rajesh Jadha | 2021 | IN202121042889 |
| **16.** | Apomorphine formulation : a controlled and extended release | Francesco Trotta, Alessandro, Mauro, Roberta Cavalli, Lorenzo Priano, Stefania Cattaldo | 2022 | WO2022223522A1WIPO (PCT) |
| **17.** | A method for creating a topical gel with nanosponges to treat psoriasis more effectively | Sherbudeen Shakila, Dr. Tiruchirappalli, Ismail, Abdulrahim Mohamed, Prof. Dr., Tiruchirappalli, Mehta, Farhad,Monisha, Janarthanan | 2023 | DE202023101573U1Germany |

The preparation of dextrin nanosponges which includes the steps of preparation of dextrin solution by dissolving it in a basic solution have a pH≥10.Thus, preparing a cross-linking agent solution by dissolving a polyfunctional cross-linking agent in a water-impermeable organic solvent, and bringing the cross-linking agent solution and dextrin solution are been summarized in the above patent. Also, the above-mentioned patent provides the data one of the kinds of nanosponges that composites of sound-absorbing board and its application, belonging to sound-absorbing material field. The invention mentioned in the application of nanosponge in air purification states that an exhaust gas purification system for a tunnel, which is distinguished by having sequentially placed negative ion purification devices on two sides of the tunnel, sequentially placed air purification devices at the top of the tunnel, and sequentially placed exhaust purification devices on the ground of a tunnel exhaust outlet. The invention relating about application of nanosponges as a vehicle of pharmaceutical formulation comprising of the cyclodextrin nanosponges which acts a vehicle for antitumoral drugs which are insoluble in water. The silicon nanosponges are prepared from a metallurgical grade silicon powder having an initial particle (10) size ranging from about 1 micron to about 4 microns. The invention mentioned for metallic coated nanoparticles states that novel metallic nanoparticles are coated with a thin protective carbon shell, and three-dimensional nano-metallic sponge and its uses which includes wood preservation, strengthening of polymer and fiber/polymer building materials, and catalysis. The cyclodextrin nanosponges which acts as a carrier the invention is all about the use of nanosponges as carriers for enzymes, antibodies, proteins, vaccines and macromolecules. The invention about the formulation for controlled and extended release containing at least one apomorphine-loaded nanosponge made of: apomorphine or its pharmaceutically acceptable salt; and a cross-linked polymer made of either dextrin or amaltodextrin. The methods used to process licoflavone nanosponges are likewise included in the invention also inventions of licoflavone nanosponges have a high rate of licoflavone dissolution and bioavailability, which enhance patient compliance and guarantee clinical efficacy. The invention related to the technical disciplines of electrode materials, specifically a type of nanosponges carbon composite Cu2O and Cu flexible electrode. requisites and planning. Reconstitutable hydrogel powder of dapsone nanosponges for the treatment of acne are the subject of the current invention. Consisting of preservatives, raw donkey milk, porous nanosponges creating pharmaceutically acceptable polymers, and dapsone. The invention about the synthesis of a gel for the treatment of psoriasis and the technique for creating a topical gel that is laden with nanosponges for improved psoriasis treatment is the focus of patent relating to nanosponge related to topical gel. The etoricoxib nanosponges loaded hydrogel primarily consists of etoricoxib loaded nanosponges made using the emulsion solvent diffusion method. The creation of cross linked nanoporous Nanosponge material will be possible through the reaction of saccharides with cross-linkers in a single pot at various saccharides to cross-linker ratios. The employment of suitable cross-linkers and surface grafting agents allows for the introduction of new functional groups onto this material. The crosslinking nano-porous carbohydrate material that uses carbohydrates as its structural building blocks material also the presence of nano-pores or nano-cavities, the nano-porous nano-sponge material has a larger inner surface area and can be widely applied to the aspects of heat insulation, water retention, hydrophobic finishing, deodorization, metal ion exchange or absorption from water or soil, and similar processes. The template polymer free nanosponges invention is successful in offering a straightforward, single-step procedure producing porous, low density, high surface area metal nanosponges which have strong anti-bacterial action and were discovered to be effective self-supported substrates for surface-enhanced Raman spectroscopy (SERS).

**CONCLUSION**

The original purpose of nanosponge was to deliver medications topically. They are the latest discoveries of colloidal carriers and recommended for administering drugs while their application may solubilize poorly water soluble medications and give delayed release as well as enhancing drugs bioavailability and in certain cases also changes its pharmacokinetics parameters. As potential substitutes for targeted drug delivery, nanosponge-based systems with exceptional porosity, straightforward functionalization procedures, distinctive topologies, and cost as well as eco-effectiveness have been investigated. The pharmaceutical industry will benefit considerably when clinical trials are able to demonstrate that medications delivered by nanosponges are safe for use in humans. Future research should focus on effectively functionalizing nanosponges to reduce potential toxicity, improve their biosafety, and increase their specificity and selectivity.

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